Assessment of LVEF using a new 16-segment wall motion score in echocardiography

Real Lebeau MD¹, Karim Serri MD¹, Maria Di Lorenzo MD¹, Claude Sauvé MD¹, Van Hoai Viet Le MD¹, Vicky Soulîères MD¹, Malak El-Rayes MD¹, Maude Pagé MD¹, Chimène Zaïani MD¹, Jérôme Garot MD² and Frédéric Poulin MD MSc¹

¹Hôpital du Sacré-Coeur de Montréal, Université de Montréal, Montréal, Canada
²Institut cardiovasculaire Paris Sud, Massy, France

Correspondence should be addressed to R Lebeau: real.lebeau@yahoo.ca

Abstract

Background: Simpson biplane method and 3D by transthoracic echocardiography (TTE), radionuclide angiography (RNA) and cardiac magnetic resonance imaging (CMR) are the most accepted techniques for left ventricular ejection fraction (LVEF) assessment. Wall motion score index (WMSI) by TTE is an accepted complement. However, the conversion from WMSI to LVEF is obtained through a regression equation, which may limit its use. In this retrospective study, we aimed to validate a new method to derive LVEF from the wall motion score in 95 patients.

Methods: The new score consisted of attributing a segmental EF to each LV segment based on the wall motion score and averaging all 16 segmental EF into a global LVEF. This segmental EF score was calculated on TTE in 95 patients, and RNA was used as the reference LVEF method. LVEF using the new segmental EF 15-40-65 score on TTE was compared to the reference methods using linear regression and Bland–Altman analyses.

Results: The median LVEF was 45% (interquartile range 32–53%; range from 15 to 65%). Our new segmental EF 15-40-65 score derived on TTE correlated strongly with RNA-LVEF ($r = 0.97$). Overall, the new score resulted in good agreement of LVEF compared to RNA (mean bias 0.61%). The standard deviations (s.d.s) of the distributions of inter-method difference for the comparison of the new score with RNA were 6.2%, indicating good precision.

Conclusion: LVEF assessment using segmental EF derived from the wall motion score applied to each of the 16 LV segments has excellent correlation and agreement with a reference method.

Key Words

- left ventricular ejection fraction
- transthoracic echocardiography
- wall motion score
- radionuclide angiography

Introduction

Two-dimensional transthoracic echocardiography (TTE) is a useful non-invasive method for estimating left ventricular (LV) volumes and left ventricular ejection fraction (LVEF). The recommended Simpson biplane method of disks has intrinsic limitations such as its dependence on geometric assumptions and the limited number of views used to derive global LVEF (1). Radionuclide angiography is a reference method with less operator dependency and excellent interobserver variability but involves exposure to ionizing radiation (2). Cardiac magnetic resonance imaging (CMR) is the gold standard for the precise estimation of LV volumes and
LVEF requiring meticulous tracings of endocardial borders in short-axis planes (3). Using TTE, wall motion score index (WMSI) can be derived and used as an alternative for evaluating LVEF (1). However, the conversion from a WMSI to LVEF is obtained through a regression equation, which may limit its routine use. In this retrospective study, we aimed to validate a new method to derive LVEF from the wall motion score in 95 patients undergoing TTE.

Methods

Patient selection

We included 95 randomly selected patients who underwent both TTE and radionuclide angiography (RNA). Patients with poor diagnostic quality of echocardiographic images or LVEF greater than 65% (by RNA) were excluded. Furthermore, patients with severe valvular disease, hypertrophic cardiomyopathy or congenital heart disease were also excluded. Consent has been obtained from each patient after full explanation of the purpose and nature of all procedures used. The study protocol was approved by the Hôpital du Sacré-Cœur de Montréal Research Ethics Board.

Echocardiography

Transthoracic echocardiograms and Doppler studies were performed in accordance with the American Society of Echocardiography (ASE) guidelines. All standard parasternal long- and short-axis as well as apical views were used to qualitatively derive the classical wall motion score (1). RNA and TTE were performed within three days of one another. The technique used to perform RNA was detailed previously (4). Visual semi-quantitative assessment of regional wall motion and thickening for wall motion score was performed by an experienced cardiologist in a blinded fashion. Wall motion score was transposed to a graphic representation of the cardiac polar map (Fig. 1). WMSI was also converted to LVEF through a validated regression equation (LVEF=0.93−(0.26×WMSI)) (Table 1) (4).

New segmental EF 15-40-65 score

The new score consisted of attributing a segmental ejection fraction (EF) to each of the LV segments based on the wall motion score and averaging all 16 segmental EFs into a global LVEF. It was derived from the standard regional wall motion assessment using a 16-segment LV model (6 basal, 6 mid and 4 apical segments) as recommended by the ASE.
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The new score relies on a correspondence between a segmental wall motion score and a segmental EF defined as follows: normokinesia (EF = 65%), hypokinesia (EF = 40%) and akinesia (EF = 15%), corresponding respectively to normal motion and normal thickening, reduced motion and thickening and absence of motion and thickening of the segment. Hypokinesia was further subdivided into mild hypokinesia (EF = 50%) and severe hypokinesia (EF = 30%). Dyskinetic (systolic bulging) and aneurysmal (systolic and diastolic bulging deformation) segments were attributed EF = 0%. In this simplified score, hyperkinesia was considered equivalent to normokinesia. The global LVEF was obtained by averaging all 16 segmental EF into a global LVEF (Fig. 1).

**Intraobserver and interobserver variability**

Twenty randomly selected studies were reanalyzed by the same operator several months after the initial analysis. A second experienced observer, also blinded to previously obtained data, analyzed the same loops for the assessment of interobserver variability of the wall motion score.

**Statistical analysis**

Categorical variables are expressed in frequency and percentages. Normality of distribution of continuous variables is assessed with the Shapiro–Wilk test. Continuous variables are described as mean ± standard deviation (s.d.) if the distribution was normal, otherwise as median and interquartile range (IQR) (25th–75th). LVEF derived using the new segmental EF 15-40-65 score was compared with the reference method using linear regression and Bland–Altman analysis.

Using Bland–Altman analysis, we evaluated systematic bias (using mean differences between methods), s.d. of inter-method difference and precision (range within which are 95 of values of differences between methods, i.e. ±1.96s.d. of differences between methods) (5). The intraobserver and interobserver variability were evaluated with the intraclass correlation coefficient. All statistical analyses were conducted using SPSS, version 24 (SPSS). When applicable, a two-tailed P value of 0.05 was used for all analysis.

**Results**

Our cohort consisted of 95 individuals (mean age 69, range 21–88 years, 42% female) with a median RNA-LVEF of 45% (IQR 30–59%; range from 15 to 65%). Ischemic cardiomyopathy (n = 72; 75%) was the most common diagnosis followed by dilated cardiomyopathy (n = 14; 15%).

**Validation of the new segmental EF 15-40-65 score**

The median LVEF obtained by the new segmental EF 15-40-65 score was 43% (IQR 28–56; range from 20

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**Table 1** The conversion of echo and CMR WMSI into LVEF by regression models in three studies of 1132 patients.

<table>
<thead>
<tr>
<th>WMSI</th>
<th>Reference LVEF methods</th>
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<tbody>
<tr>
<td></td>
<td>RNA-LVEF⁺ (N=243) (4)</td>
</tr>
<tr>
<td>1.0</td>
<td>67</td>
</tr>
<tr>
<td>1.1</td>
<td>65</td>
</tr>
<tr>
<td>1.2</td>
<td>62</td>
</tr>
<tr>
<td>1.3</td>
<td>61</td>
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<tr>
<td>1.4</td>
<td>57</td>
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<td>1.5</td>
<td>54</td>
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<td>1.6</td>
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<td>50</td>
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<td>1.8</td>
<td>47</td>
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<td>1.9</td>
<td>44</td>
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<td>2.0</td>
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<td>2.7</td>
<td>24</td>
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<tr>
<td>2.8</td>
<td>21</td>
</tr>
<tr>
<td>2.9</td>
<td>18</td>
</tr>
<tr>
<td>3.0</td>
<td>15</td>
</tr>
</tbody>
</table>

⁺WMSI calculated using the transthoracic echocardiogram; †Semi-quantitative echo LVEF was defined as the combination of the modified method of Quinones combined with an overall visual estimation of LVEF; ‡WMSI calculated using the cardiac magnetic resonance.
to 65%). The correlation between RNA-LVEF and the new segmental EF 15-40-65 score was excellent ($R = 0.97$) (Fig. 2).

**Analysis of systematic bias**

Bland–Altman analysis showed excellent agreement between the new score and RNA (mean LVEF bias = 0.61%) (Fig. 3 and Table 2). Linear regression analysis confirmed the absence of proportional bias.

**Analysis of precision**

The s.d. of the distribution of inter-method differences between the new score and RNA-LVEF were acceptable. The s.d. was ±3.17% (±7% of the median RNA-LVEF). Consequently, the 95% confidence interval of inter-method difference (±1.96×s.d. i.e. precision) was 12.4% (Fig. 3 and Table 2).

Assessment of LVEF using the regression-based method from the classic wall motion score was not superior to the new segmental EF 15-40-65 score showing equivalent correlation vs RNA-LVEF ($R = 0.97$) and similar accuracy and precision (Supplementary Table, see section on supplementary data given at the end of this article).

**Reproducibility**

Analysis of intraobserver and interobserver variability for the wall motion score demonstrated good agreement between observations (intraobserver 0.97; interobserver 0.97).

**Discussion**

In this study of patients with a broad range of LVEF referred for TTE, we aimed to test the validity of a simplified method to convert segmental wall motion assessment into segmental EF to easily obtain the global LVEF. The main results were:

1. The use of the new segmental EF (15-40-65) score resulted in excellent correlation and excellent systematic bias overall compared with reference LVEF methods.
2. Precision of this new score by echocardiography to assess LVEF was clinically acceptable compared with a reference method.

**Classical WMSI**

The WMSI has been previously validated in several echocardiographic studies and well correlated with RNA-LVEF (6, 7). We published in 2003 an assessment of LVEF derived from WMSI in 243 patients using the classical
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Table 1

<table>
<thead>
<tr>
<th>RNA-LVEF vs segmental EF 15-40-65 score on TTE</th>
<th>Mean difference between methods ± s.d. (%)</th>
<th>Precision (%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>LVEF, left ventricular ejection fraction; RNA, radionuclide angiography.</td>
<td>0.61 ± 3.17</td>
<td>12.4</td>
</tr>
</tbody>
</table>

16-segment model, as recommended by the ASE (4). We obtained an excellent correlation ($r=0.88$) and agreement with RNA-LVEF in all stratum of LVEF. The regression equation derived was RNA EF = 0.93 – (0.26 x WMSI), which has been reproduced thereafter by Moller et al. from the Mayo Clinic using TTE (8) and by Lebeau et al. on CMR (9) in a total of 1132 patients (Table 1). In a study of 110 patients by Duncan et al. comparing echocardiographic LVEF derived from the WMSI, echocardiographic Simpson’s biplane method and LVEF obtained by CMR, WMSI-derived LVEF had a stronger correlation with CMR than Simpson’s biplane method and was more accurate (10). In a systematic review by McGowan et al. WMSI-LVEF has proven to be a valid method to assess LVEF (11), potentially superior to Simpson’s biplane method. Similarly, in a CMR study involving 203 patients, Sierra-Galan et al. have demonstrated that the WMSI is an accurate method to measure LVEF (12) and is a useful complement to automatic border detection that can often be erratic.

We believe that the WMSI model has several advantages over the planimetric method. The WMSI method takes advantage of the multiple incidences of the LV to complete a polar map as opposed to only two sagittal views used for the classical Simpson’s biplane method. The Simpson formula is also less precise in patients with very abnormal ventricular geometry (dyskinesia or aneurysm) (1). In the setting of acute myocardial infarction, WMSI reflects the size of myocardial infarction better than LVEF (13, 14, 15). WMSI is also superior to LVEF for risk stratification (death and re-hospitalization for heart failure, re-MI, stroke) after acute myocardial infarction (8, 16, 17, 18, 19).

Simplified wall motion score

We have previously shown that a semi-quantitative method dedicated specifically to emergency and critical care physicians based on the simple assessment of normokinesia (EF = 60%), hypokinesia (EF = 40%) or akinesia (EF = 20%) in the 3 short-axis views was superior to global visual estimation (20, 21). In the current study, we applied the new segmental EF 15-40-65 score in TTE to each of the 16 segments of the polar map and obtained a global LVEF resulting from the arithmetic mean of all segmental EF. The rationale behind this segmental EF using WMS is the strong linear relation between WMSI and LVEF (4, 8, 9). Indeed, in previous studies of global LVEF, the global WMSI was translated into LVEF by a mathematical regression model (Table 1) (4, 8, 9). For instance, a normal LV function with no wall motion abnormalities has a score of 1.0 corresponding to an LVEF of 67% and CMR LVEF of 64% (65% was used as mean approximation). Mild diffuse hypokinesia with a score of 1.5 has an echo LVEF of 54% and CMR LVEF of 51% (mean approximation = 50%). Diffuse hypokinesia with a score of 2 has an echo LVEF of 41% and CMR LVEF of 38% (mean approximation = 40%). Severe diffuse hypokinesia with a score of 2.5 has an echo LVEF of 28% and CMR LVEF of 25% (mean approximation = 30%). Diffuse akinesia has an echo LVEF of 15% and CMR LVEF of 12% (mean approximation = 15%). We simply assigned a segmental EF for each segment based on the aforementioned convention, translating segmental wall motion score into a segmental EF and then obtained global LVEF by averaging the 16-segment EF.

This new method to derive global LVEF was accurate compared to a reference method. We consider that the precision obtained (12%) with this new segmental EF 15-40-65 score was reasonable. Indeed, it compares favorably to the precision of three-dimensional echocardiography compared with CMR in a meta-analysis (precision of 3D = 24%) (22) and in the more recent study of Hoffmann et al. (precision of 3D = 48%) (23). Thus, the use of this simple and highly reproducible method to easily obtain global LVEF from the bull’s eye representation of wall motion score using all standard views, which has not been described before, has the potential to refine the daily assessment of systolic function in busy echocardiography laboratories and at the bedside by sonographers and cardiologists.

Perspectives of wall motion score

It is becoming accepted that strain and 3D have superior sensitivity and reproducibility to detect LV systolic dysfunction (1). However, they require more expertise and several technical pitfalls and standardization issues
remain. With the widespread utilization of portable and handheld echocardiography in emergency departments and intensive care units to evaluate patient hemodynamics, LV wall motion assessment is an easier method to assess LV systolic function and is generalizable to a wider range of physicians with various level of training, expertise and echocardiographic equipment (24, 25, 26). We have shown herein that a simple segmental score (EF 15-40-65) applied to each of the 16 segments results in a robust estimation of LVEF by echocardiography.

**Limitations**

The most significant limitation remains the capacity to obtain good images and sufficient ability to interpret motion abnormalities. The wall motion scores were assessed by an experienced echocardiographer. While we acknowledge that estimation of the wall motion abnormalities can be subjective, our interobserver variability was very acceptable. In cases where there is discrepant wall motion score in a given segment, we believe that short-axis parasternal views should be weighted more heavily in the final score of that segment. Indeed, short-axis views offer the only real 3D (360°) analysis of cardiac dynamics as opposed to the limited degrees of evaluation obtained with the thin sagittal cuts from the apical views.

This model of wall motion score is not designed for the evaluation of hyperkinetic states, because the maximal score by our semi-quantitative model is 65%. This model should be reserved for patients with LV dysfunction and used cautiously in patient with localized hyperkinetic wall motion since it will result in an underestimation of LVEF. Whether this new score can be extrapolated to a 17-segment model is likely but remains to be validated. The apical cap is a small segment with little intrinsic kinesis and is more useful to assess in perfusion studies. Additionally, attributing a segmental EF score of 0% to dyskinetic or aneurysmal segments was preferred to a negative correction (for example, segmental EF of −15%) since the latter would have led to systematic underestimation of LVEF in exploratory analyses of 11 patients with such segmental abnormalities. Finally, improving endocardial definition in TTE with the use of contrast agents could have resulted in improved precision of the new segmental EF 15-40-65 score (27).

**Conclusion**

Our results suggest that the estimation of LVEF using a new segmental EF 15-40-65 score is an accurate method and a good complement to planimetric methods. Any echocardiography laboratory that systematically assesses LV function by grading the wall motion score (16-segment model) can then easily translate this routine information into a robust estimate of LVEF without the use of regression equations.

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**Supplementary data**

This is linked to the online version of the paper at https://doi.org/10.1530/ERP-18-0006.

**Declaration of interest**

The authors declare that there is no conflict of interest that could be perceived as prejudicing the impartiality of the research reported.

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