REVIEW

The modern role of transoesophageal echocardiography in the assessment of valvular pathologies

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Abstract

Despite significant advancements in the field of cardiovascular imaging, transoesophageal echocardiography remains the key imaging modality in the management of valvular pathologies. This paper provides echocardiographers with an overview of the modern role of TOE in the diagnosis and management of valvular disease. We describe how the introduction of 3D techniques has changed the detection and grading of valvular pathologies and concentrate on its role as a monitoring tool in interventional cardiology. In addition, we focus on the echocardiographic and Doppler techniques used in the assessment of prosthetic valves and provide guidance for the evaluation of prosthetic valves. Finally, we summarise quantitative methods used for the assessment of valvular stenosis and regurgitation and highlight the key areas where echocardiography remains superior over other novel imaging modalities.

Introduction

Over the past decade, advancements in transoesophageal echocardiography technology (TOE) have expanded the clinical applications of TOE beyond that of a purely diagnostic tool for assessing the valvular pathology. The latest TOE probes offer exceptional image quality and high resolution. The introduction of real-time 3D TOE transducers and hybrid imaging techniques have revolutionised its role as an excellent monitoring tool in the cath lab and in the peri-operative period. The use of 3D-capable transducers allows more complex data processing and measurements of curved areas of valvular structures as well as accurate visualisation of regurgitant jets. Real-time three-dimensional echocardiography is changing the practice of cardiology.

The echocardiographic assessment of patients undergoing transcatheter assessment differs from those of the routine evaluation of patients with native and prosthetic valves. TOE plays an essential role in the initial assessment, in the intra-procedural monitoring of device deployment and function and is the primary modality in the assessment of procedural complications and follow-up.

Here, we provide an overview of recommendations how to assess valvular pathologies using established transoesophageal 2D and 3D methods.

Current role of TOE in management of valvular heart disease

The significance of a systematic approach in performing every transoesophageal examination cannot be
emphasised strongly enough. The recent guidelines developed by the British Society of Echocardiography (BSE) provide a framework for performing a standardised TOE in any clinical settings (1, 2). This is particularly important when assessing valvular pathologies because the judgement of the severity depends on the assessment of size and function of both ventricles and concomitant pathologies, which may alter the physiology.

**Mitral regurgitation**

Mitral regurgitation (MR) is the most common cause of valvular regurgitation in the Western countries and is the best example how the introduction of 3D TOE has changed how we manage this disease.

**MR classification**

MR is classified as either primary (organic) or secondary (functional) in origin. Conventional 2D TOE requires multiple views of the mitral valve (MV) and use of the Doppler in defining the aetiology of MR. The best known classification of MR was proposed by Carpentier in the 1980s. It is based on the key differences in the leaflet motion. In type I, lesions are characterised by normal leaflet motion, and MR is a result of mitral annular dilatation or leaflet perforation (centrally directed jet). In type II, MR results from elongated or ruptured chordae allowing the affected leaflet to move beyond the coaptation line (jet is directed away from the prolapsing or flail leaflet). In type III, MR is a result of restricted leaflet motion and can be differentiated further into IIIa and b categories, which describe the type of restriction as either during both systole and diastole (rheumatic MR) or only in the systole as observed in ischaemic cardiomyopathy and caused by apical displacement of papillary muscles (jet directed towards the restricted leaflet). Examples of MV pathologies are shown in Videos 1, 2, 3, 4.

**Echocardiographic assessment of MR**

The European Association of Echocardiography (EAE) recommends transthoracic echocardiography (TTE) as the first line in the assessment of MR (3) and suggests that the complete examination should include analysis of aetiology of MR, the assessment of the mechanism and severity of MR and the likelihood of valve repair. Although frequently used in cases of severe MR, TOE is recommended peri-operatively and in cases when

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**Video 1**


**Video 2**


**Video 3**


**Video 4**


TTE cannot give the definitive answer regarding the mechanism of regurgitation and the suitability for repair (3). According to the EAE TOE update from 2010 (4), essential views for MR analysis involve transgastric basal short axis view allowing localisation of the origin of the jet and visualisation of six scallops and two commissures, multiple mid-oesophageal views for systematic analysis of scallops, papillary muscles and chordae and colour Doppler assessment of the regurgitant jet and pulsed-wave Doppler of the upper pulmonary veins.

The echocardiographic assessment of the severity of MR is based on multiple parameters (vena contracta, PISA method and the analysis of pulmonary vein flow), which are described in detail in Table 1.

**Pitfalls**

It is important to note that general anaesthesia and sedation may significantly alter the loading conditions of the circulation and that this must always be taken into account when grading MR using TOE. A reduction in ventricular filling, systemic vascular resistance and blood pressure may all lead to a systematic underestimation of the degree of MR. Moreover, when judging the severity of MR and the suitability for repair or replacement, the LV response to the valve lesion must be assessed by taking into account the ejection fraction (<60%) and LV end-systolic diameter (>45 mm; less load dependent than end diastolic volume) (5). A recent large multicenter study
showed a better survival rate in patients operated on before the LV end-systolic diameter reached 40mm (6). As the LV response has been shown to be of prognostic significance, further research has focused on identifying more sensitive echocardiographic markers of subclinical LV dysfunction, such as longitudinal strain and tissue Doppler; although some studies suggest that they may be of some value, they have not yet entered routine clinical practice (7, 8).

**Mitral valve repair**

Mitral valve repair has been widely accepted as a preferential method of management of MR. This strategy is supported by better long-term outcomes as a result of preservation of the chordal attachments, low rates of thromboembolism, no need for lifelong anticoagulation and very good durability. A recent meta-analysis showed that a strategy of early mitral valve repair in asymptomatic severe MR is superior when compared with a strategy of ‘watchful waiting’ (9). Although controversy remains, the guidelines suggest consideration of earlier intervention in cases suitable for repair (10, 11).

MV repair is feasible in 95% of patients with degenerative valve disease, 70% with rheumatic valve disease and 75% with ischaemic valve disease (12). Optimal results are anticipated in cases with isolated posterior leaflets (P2) prolapse, but is significantly reduced in cases of anterior commissural prolapse, multiple prolapsing scallops, severe mitral annular dilatation (>50mm), extensive MV calcification, large central

### Table 1  
Echocardiographic parameters used for the determination of the severity of valvular regurgitation as per EACVI (19) and the British Society of Echocardiography (BSE) guidelines.

<table>
<thead>
<tr>
<th>Severe regurgitation</th>
<th>Quantitative parameters</th>
<th>Doppler parameters</th>
<th>Strong predictors</th>
<th>Haemodynamic consequences</th>
</tr>
</thead>
<tbody>
<tr>
<td>Mitral</td>
<td><strong>Organic MR</strong>&lt;br&gt;VC width (cm) &gt;0.7&lt;br&gt;R Vol (mL/beat) &gt;60&lt;br&gt;RF (%) &gt;50&lt;br&gt;EROA (cm²) ≥0.40</td>
<td>Colour flow jet area: large central jet or eccentric jet adhering, swirling and reaching the posterior wall of the LA</td>
<td>Systolic flow reversal in pulmonary veins</td>
<td>LA and LV dilated</td>
</tr>
<tr>
<td></td>
<td><strong>Ischaemic MR</strong>&lt;br&gt;R Vol (mL/beat) &gt;30&lt;br&gt;EROA (cm²) ≥0.20</td>
<td>Mitral inflow: dominant E wave &gt;1.5 m/s</td>
<td>Jet density, CW: dense, triangular, early peaking</td>
<td>Holodiastolic flow reversal in the upper part of descending and in abdominal aorta</td>
</tr>
<tr>
<td>Aortic</td>
<td>VC width (cm) ≥0.6&lt;br&gt;Jet width/LVOT width: &gt;6&lt;br&gt;R Vol (mL/beat): ≥60&lt;br&gt;RF (%): &gt;50&lt;br&gt;EROA (cm²): ≥0.30</td>
<td>Jet width in LVOT-colour flow: large in central jets, variable in eccentric jets</td>
<td>Jet density, CW: dense</td>
<td>LA and LV dilated</td>
</tr>
<tr>
<td></td>
<td>Jet density, CW: dense</td>
<td>Jet deceleration area (PHT, ms): steep &lt;200</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Tricuspid</td>
<td>VC width (cm) &gt;0.7&lt;br&gt;PISA radius (cm) &gt;0.9 at a Nyquist limit of 28 cm/s</td>
<td>Jet area, central jets (cm²): &gt;10</td>
<td>Systolic flow reversal in hepatic veins</td>
<td>RA, RV, IVC dilated</td>
</tr>
<tr>
<td>Pulmonary</td>
<td>VC width, EROA, R Vol not defined</td>
<td>Jet size by colour Doppler: large with a wide origin, may be brief in duration</td>
<td>Systolic flow reversal in pulmonary arteries</td>
<td>RV dilated</td>
</tr>
<tr>
<td></td>
<td>Jet density, CW: dense, steep deceleration, early termination of diastolic flow</td>
<td>Pulmonic systolic flow compared to aortic flow-PW: greatly increased</td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

CW, continuous-wave; ERO, effective orifice area; LA, left atrium; LV, left ventricle; PHT, pressure half time; PW, pulse-wave; RA, right atrium; RF, regurgitation fraction; RV, right ventricle; R Vol, regurgitation volume; VC, vena contracta.
regurgitation jet and in other forms of primary MR secondary to endocarditis or rheumatic disease (3). Hence, the detailed echocardiographic assessment is crucial in the management of MR.

2D TOE had a transformative impact on the surgical treatment of mitral valve pathology in the 1980s enabling acquisition of high-quality views of the mitral valve allowing the repair strategy to be determined pre-operatively, the efficacy of the repair to be assessed, and immediately corrected post-operatively if necessary. Several decades later, advances in transducer technology have enabled acquisition of 3D and 4D anatomical imaging providing more detailed information relating to valve morphology and dynamics. The promise of these new technologies is to increase the precision of mitral valve diagnostics to tailor the repair plan to an individual’s valve pathology. There is also hope that 3D and 4D TOE will be able to predict the outcome of a given repair technique using image-derived valve models as input to computational biomechanical analysis and by optimizing annuloplasty ring design.

Echocardiographic parameters of suitability for MV repair

There are no widely accepted criteria for establishing the suitability for MV repair, and the decision is based on the anatomical lesion and the experience of the surgeon. The echocardiographic report should include the degree of MR and MS, the specific location of prolapsing or flail leaflet segments, the presence of leaflet perforation, calcification, excessive length and thickening of the leaflet and areas of normal leaflet mobility. The subvalvar apparatus should be assessed for the presence of torn chordae and chordal thickening. Additionally, the haemodynamic consequences of MR should be described as follows: the presence of a dilated left atrium with or without thrombus, the size and function of both ventricles and the presence of other significant valvular pathologies. Moreover, the surgeon should be alerted if there is a risk for systolic anterior motion of the MV with resultant left ventricle outflow obstruction after the MV repair.

Echocardiographic assessment for MitraClip

Percutaneous mitral valve edge-to-edge repair has evolved into a therapeutic option for high surgical risk patients with severe functional MR as well as insufficiency secondary to prolapse or flail leaflet (13). Several parameters (mostly derived from the Everest II trial (14, 15)), as defined in Table 2, can be assessed to predict the success of the procedure. Although very useful in the assessment of suitability for the procedure, the majority of centres will rely on a case-by-case assessment. The TOE should assess the MV morphology, the grade and the cause of the MR. The ideal valve morphology for a MitraClip procedure includes: degenerative or functional MR, no calcification in the grasping area, MVA >4 cm², length of the posterior leaflet coaptation length and depth >2 mm and <11 mm respectively, Gap between leaflets <10 mm, Width of flail leaflet <15 mm, Mitral valve opening area >4 cm², Leaflet thickness <5 mm, Considerable calcification of the mitral annulus Not present, Marked restriction of posterior leaflet Not present, Lack of primary or secondary chordal support Not present, Several significant regurgitates jets Not present, Procedural steps guided by echo during Mitral Clip

The trans-septal puncture 3.5 cm to 4 cm above the plane of the mitral annulus, The advancement of the dilator though the interatrial septum The navigation of the clip-delivery-system in the left atrium towards the mitral valve The positioning of the device within the mitral leaflet zone of prolapse or coaptation defect The adjustment of perpendicularity of the clip into the left ventricle The grasping of the anterior and posterior leaflet by the clip and the closure of the clip Echo assessment post procedure Mitral Clip

Reduction of the mitral valve regurgitation Exclusion of the mitral stenosis

Table 2  Echocardiographic analysis of the mitral valve prior, during and post Mitral Clip procedure using Everest criteria.

<table>
<thead>
<tr>
<th>Echo assessment prior to Mitral Clip</th>
<th>Procedural steps guided by echo during Mitral Clip</th>
<th>Echo assessment post procedure Mitral Clip</th>
</tr>
</thead>
<tbody>
<tr>
<td>Mitral leaflet coaptation length and depth</td>
<td>The trans-septal puncture</td>
<td>Reduction of the mitral valve regurgitation</td>
</tr>
<tr>
<td>Gap between leaflets</td>
<td>The advancement of the dilator though the interatrial septum</td>
<td>Exclusion of the mitral stenosis</td>
</tr>
<tr>
<td>Width of flail leaflet</td>
<td>The navigation of the clip-delivery-system in the left atrium towards the mitral valve</td>
<td></td>
</tr>
<tr>
<td>Mitral valve opening area</td>
<td>The positioning of the device within the mitral leaflet zone of prolapse or coaptation defect</td>
<td></td>
</tr>
<tr>
<td>Leaflet thickness</td>
<td>The adjustment of perpendicularity of the clip into the left ventricle</td>
<td></td>
</tr>
<tr>
<td>Considerable calcification of the mitral annulus</td>
<td>The grasping of the anterior and posterior leaflet by the clip and the closure of the clip</td>
<td></td>
</tr>
<tr>
<td>Marked restriction of posterior leaflet</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Lack of primary or secondary chordal support</td>
<td></td>
<td></td>
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<tr>
<td>Several significant regurgitates jets</td>
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<tr>
<td>&gt;2 mm and &lt;11 mm respectively</td>
<td>3.5 cm to 4 cm above the plane of the mitral annulus</td>
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<tr>
<td>&lt;10 mm</td>
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<tr>
<td>&lt;15 mm</td>
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<tr>
<td>&gt;4 cm²</td>
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<tr>
<td>&lt;5 mm</td>
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<tr>
<td>Not present</td>
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<td>Not present</td>
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<td>Not present</td>
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<tr>
<td>Not present</td>
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</tbody>
</table>

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leaflet \(\geq 10\) mm, flail-gap \(< 10\) mm and sufficient leaflet tissue for mechanical coaptation (16). On the other hand, perforated mitral leaflets, lack of chordal support, severe calcification in the grasping area and the presence of mitral stenosis especially rheumatic in origin makes the MR unsuitable for MitraClip. 3D TOE offers a remarkable benefit here allowing en face views of the MV from both LV and LA perspective. It provides a detailed description of the anatomy and function of the MV, the mitral valve apparatus and the structures in proximity to the MV (left atrial appendage and the aortic and tricuspid valves). Moreover, TOE plays a crucial role in guiding such key steps in MitraClip procedure as: (1) transseptal puncture, (2) introduction of guide catheter, (3) advancement of the delivery system, (4) positioning of the MitraClip and (5) grasping of the leaflets. There is a hope the combined methods using echocardiography and fluoroscopy fusion imaging will improve the success rate in the future.

**Mitral valve stenosis**

The most common aetiology of mitral stenosis (MS) is rheumatic heart disease (17); the appearance of the valve is characterised by commissural fusion, chordal shortening and leaflet thickening and superimposed calcification contributing to the restriction of leaflet motion (18). Another pathognomonic feature of rheumatic MS is a hockey stick appearance of the anterior leaflet of the mitral valve caused by thickening of the leaflet tips. The transgastric two-chamber view is particularly helpful in the assessment of the subvalvular apparatus in more advanced cases when calcification of leaflets and annulus becomes apparent. All these echocardiographic findings need to be taken into consideration when grading the severity of MS and making a decision regarding suitability for balloon mitral commissurotomy. In patients undergoing mitral valvuloplasty for MS, the Wilkin’s scoring system is used to predict the outcome (19). Leaflet mobility, valve thickening, calcification, subvalvular thickening and commissural calcification or fusion are taken into account when predicting the outcome. Additionally, 3D echocardiography allows visualisation of the mitral valve from both the left atrial and the ventricular perspective and improves the ability to perform an accurate en face mitral valve planimetry by allowing positioning of the cropping lines parallel to the narrowest orifice of the MV (Fig. 1). Zamorano and coworkers also confirmed that the real-time 3D echocardiography is feasible, accurate and highly reproducible for estimating mitral valve area (MVA) in patients with rheumatic mitral stenosis when compared against gold standard, invasive Gorlin’s method (20). The real-time 3D measurements had excellent inter- and intra-observer variability and provided the best inter-observer agreement for morphologic evaluation. Thus, this methodology has been recommended for the assessment of MVA immediately after balloon valvuloplasty.

Table 3 describes methods used for the estimation of the mitral valve area in native mitral stenosis on TOE and summarises the most important limitations associated with these methods. Reduction of mitral valve area below 2.5 cm\(^2\) increases the atrioventricular pressure gradient to maintain adequate cardiac output and subsequently leads to the enlargement of the left atrium and atrial arrhythmias including atrial fibrillation and thus increases the risk of thromboembolism. Significant long-standing MS results

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**Figure 1**

A transoesophageal 3D zoom image of the mitral valve showing severe mitral stenosis. QLAB (Philips Medical System) software was used for post-processing of the 3D dataset. The anatomical MV area (MVA) measures 0.7 cm\(^2\).
in pulmonary hypertension and subsequently right ventricular hypertrophy and enlargement. A common finding in that setting is functional tricuspid regurgitation due to right ventricular pressure overload. Thus, the echocardiographic evaluation of MS needs to consider all these haemodynamic consequences and exclude the presence of thrombus in the left atrial appendage (LAA). Another important point to note is the requirement of averaging 3–5 values for the assessment of mean pressure gradient when atrial fibrillation is present.

### Aortic regurgitation

The recommendations from the European Association of Cardiovascular Imaging (EACVI) regarding echocardiographic assessment of aortic regurgitation (AR) suggest that the echo report should include information about the aetiology, the type of dysfunction and the likelihood of valve repair (21). The assessment of the morphology and dimension of the aortic root is also mandatory. 3D echocardiography can provide better delineation of the valvular morphology including the description of the cusp pathology (redundancy, restriction, cusp height to indicate likely adequacy of coaptation, pliability, thickness and integrity) and commissure variations (fusion, splaying, attachment site and alignment) (22). The classification system, similar to Carpentier classification system for MR, has been developed to describe the mechanism of AR, guide repair techniques and allow long-term follow-up. The key in understanding the aetiology of AR is the distinction between the intrinsic disease of the aortic cusps (calcific, rheumatic, myxomatous, congenital, infectious or traumatic) and the conditions that affect predominantly aortic annulus such as annular dilatation, aortic dissection and aneurysmal disease.

The grading of the severity of AR is based on parameters described in detail in Table 3. Briefly, the vena contracta, proximal isovelocity surface area (PISA) and its calculation method should be included in the echocardiographic report.

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**Table 3** Methods for calculating mitral valve area (MVA) in native mitral stenosis on TOE.

<table>
<thead>
<tr>
<th>Method</th>
<th>How to perform</th>
<th>Points for consideration</th>
</tr>
</thead>
<tbody>
<tr>
<td>Planimetry</td>
<td></td>
<td></td>
</tr>
<tr>
<td>• by 2D</td>
<td>Tracing the mitral orifice obtained from the TG basal SAX view. Contour of the inner mitral orifice including commissures when opened</td>
<td>Direct measure of MVA, flow independent. Requires technical expertise to position the measurement plane on the mitral orifice</td>
</tr>
<tr>
<td>• by 3D</td>
<td>Performed from the mid-oesophageal view. The 3D dataset is cropped by an arbitrary plane, parallel to the MV annulus and then is planimetered using post processing software</td>
<td>3D TOE more accurate than 2D. Gold standard in the assessment of MS</td>
</tr>
<tr>
<td>Pressure gradient</td>
<td>Tracing the entire envelope of the CWD spectrum of mitral inflow, from the beginning of early diastolic flow (E wave) to the end of flow due to atrial contraction (A wave). Mean gradient from the traced contour of the diastolic mitral flow. Requires averaging values over 5–10 cycles in AF</td>
<td>Influenced by heart rate, cardiac output, and associated MR</td>
</tr>
<tr>
<td>Pressure half-time (P1/2)</td>
<td>MVA (cm²) = ( \frac{220}{P1/2} )</td>
<td>Influenced by compliance of LA and LV. Severe AR underestimates severity of MS. Not accurate in diastolic dysfunction and AF</td>
</tr>
<tr>
<td>Deceleration time (DT)</td>
<td>MVA (cm²) = ( \frac{759}{DT} ) (ms)</td>
<td>The same limitations as for using P1/2 method</td>
</tr>
<tr>
<td>Continuity equation</td>
<td>MVA (cm²) = (CSA LVOT (cm²) x VTI LVOT) (cm)/VTI MV (cm)</td>
<td>Independent from flow conditions. Multiple measurements required (source of errors). Not valid in severe AR and MR</td>
</tr>
<tr>
<td>Proximal isovelocity surface area (PISA)</td>
<td>MVA = (PISA x Velocity aliasing)/peak velocity transmitral</td>
<td>Technically difficult. Multiple measurements required. Angle correction is essential. Can be used in the presence of MR</td>
</tr>
</tbody>
</table>

3D, three dimensional; AF, atrial fibrillation; AR, aortic regurgitation; CSA, cross sectional area; CWD, continuous-wave Doppler; DT, deceleration time; MR, mitral regurgitation; MVA, mitral valve area; P1/2, pressure half-time; PISA, proximal isovelocity surface area; TG SAX view, transgastric short axis view; VTI, velocity time interval.
method and assessment of flow reversal in descending aorta are used. Colour jet area is affected by the aortic and LV diastolic pressure gradient and LV compliance and therefore is only weakly correlated to the degree of AR; colour should therefore only be used for the detection and initial visual assessment of AR \(^{(21)}\). 3D assessment of the vena contracta can be used to provide a measure of the actual regurgitation orifice area \(^{(23)}\).

The guidelines recommend the use of the PISA method for the assessment of both central and eccentric jets as it provides valuable quantitative assessment of regurgitation severity as effective orifice area (EROA) and regurgitant volume (R Vol) \(^{(22)}\). Overall, the single most significant determinant of the severity of AR is the measurement of the diastolic flow reversal in the descending and abdominal aorta \(^{(24)}\). Lastly, it is worth noting that CMR plays an increasingly important role in the assessment of AR, as it can provide accurate \textit{in vivo} quantification of the regurgitation using flow mapping \(^{(25)}\), assessment of LV function and precise information about the anatomy of the thoracic aorta.

### Aortic stenosis

Management of patients with aortic stenosis (AS) relies on accurate diagnosis of the cause and stage of the disease process. The advantage of using TOE is that it offers greater confidence of aortic valve morphology and greater accuracy for planimetry of AVA at valve tips especially in patients with poor transthoracic echocardiography (TTE) windows. One of the limitations of using TOE is that it can be quite difficult to get a pressure gradient across the AV in some patients. Thus, TTE remains the mainstream technique for the assessment of patients with AS. Significantly, 2D TOE offers greater accuracy of the LVOT diameter measurement for the continuity equation and 3D TOE also allows a biplane assessment from the long-axis view to guide a short-axis slice level with the smallest orifice in funnel-shaped valves.

According to the EAE guidelines, the following parameters should be measured to assess the severity of AS: AS jet velocity, mean transaortic gradient and valve area by continuity equation (utilizing velocity-time integrals) \(^{(26)}\). Haemodynamic severity is best characterised by the high transaortic maximum velocity (or mean pressure gradient). However, some patients with AS have a low transaortic volume flow rate due to either left ventricular systolic dysfunction with a low left ventricular ejection fraction (LVEF) or due to a small hypertrophied left ventricle with a low stroke volume. In the recent guidelines published by the American Heart Association, symptomatic severe AS has been divided into three categories: (1) high-gradient AS, (2) low-flow/low-gradient AS with reduced LVEF and (3) low-gradient AS with normal LVEF or paradoxical low-flow AS \(^{(10)}\). Especially the last category of severe AS poses a diagnostic and management challenge, and guidelines stress that interventional management could be considered in that group of patients only if clinical, haemodynamic and anatomic data support valve obstruction as the most likely cause of symptoms, and the data were recorded when the patient was normotensive. Hence, a careful approach should be undertaken when evaluating these patients with echocardiography. Loading conditions influence velocity and pressure gradients; therefore, measurements of valve stenosis should always be interpreted in the clinical context.

### Imaging before, during and after transcatheter aortic valve implantation

Assessment of aortic valve anatomy, morphology and severity of aortic valve stenosis is crucial in the pre-
procedural evaluation of candidates for transcatheter aortic valve implantation (TAVI). TOE plays an important role in the assessment of the presence of bicuspid aortic valve and extensive calcification at the commissures and the tips of leaflets, which could increase the risk of complications during the TAVI procedure. For TAVI purposes, aortic annulus is measured in the aortic long-axis at the mid-oesophageal view from the hinge point of the right coronary cusp to the commissure between left and non-coronary cusp (Videos 5, 6, 7, 8, 9, 10). The diameters of the sinus of Valsalva, sinotubular junction and ascending aorta are also measured. 3D TOE has been shown to provide better assessment of the annular size in those patients whose annulus is not circular. 3D TOE-guided prosthesis sizing has been proved to lead to implantation of larger prostheses than when 2D assessment was used (27). When the accuracy of 3D TOE measurements of aortic annulus was assessed against CT and MRI, it underestimated the size of the annulus and showed greater variability than MRI (especially when correlated with increasing calcium burden) (28).

TOE is used to guide the following steps during TAVI: the aortic valve crossing, balloon dilatation and positioning and deployment of the prosthesis (Videos 5, 6, 7, 8, 9, 10). The mid-oesophageal short-axis view is usually used to visualise the catheter position at the cusp level during procedure, and deep transgastric views are used to image the prosthetic aortic valve after implantation. It also plays a crucial role in the early assessment of the result and complications of the procedure. It can define the severity and location of paraprosthetic regurgitation, which occurs in 5–20% of patients undergoing TAVI and is associated with a 2.0- to 2.5-fold increase in mortality. Other potential complications, which could be identified by TOE include: cardiac tamponade, LV failure, severe aortic regurgitation, new mitral regurgitation, aortic dissection or occlusion of the coronary ostia.

Pulmonary valve

Pulmonary regurgitation

The echocardiographic assessment of pulmonary regurgitation (PR) includes integration of data from imaging of the PV and RV and Doppler measures of regurgitation severity (Table 1). Methods used for the quantification of valvular regurgitation have not been established for estimating the grade of the PR. Additionally, the PV and the RVOT can be difficult to assess with echocardiography due to the location of the valve behind the sternum. Hence, CMR has recently emerged as a ‘gold standard’ method for the assessment of the PV and RVOT as it can not only visualise the PV but also accurately quantify the regurgitation and RV volumes and function (25).

Percutaneous pulmonary valve implantation

Percutaneous pulmonary valve implantation (PPVI) is a treatment for PR associated with residual RVOT lesion after repair of congenital heart disease (pulmonary atresia, ventricular septal defect, Tetralogy of Fallot, absent pulmonary valve, Truncus arteriosus, Rastelli-type repair of transposition and after Ross operation). Echocardiography plays an important role in the assessment of PR, the degree RV dilatation and dysfunction, RV systolic pressure from the tricuspid regurgitant jet and the RVOT gradient calculated from the velocity across the RVOT. Not infrequently transthoracic echocardiographic assessment of the RVOT and pulmonary valve are superior to TOE given the anterior location of the structures involved. Typically a multimodality approach with echo, CMR and biplane cine-angiography are required to prepare for the procedure. Similar to other interventional procedures, TOE can be used to guide the balloon positioning, the valve deployment and in the assessment of pressure gradients across RVOT to determine the success of the valve placement, although frequently it is performed under fluoroscopic control only.

Pulmonary stenosis

Pulmonary stenosis is almost always congenital in origin and echocardiography together with CMR plays important role in the assessment of these pathologies. The particular attention should be taken to exclude the RVOT obstruction from the right
ventricular hypertrophy mimicking pulmonary stenosis in selective cases. Direct planimetry of the valve cannot be performed because TOE does not allow visualisation of the pulmonary valve \textit{en face}. Assessment of the right ventricle size and function are important in grading the severity of pulmonary stenosis. Quantitative assessment is mainly based on the transpulmonary pressure gradient. Other methods have not been validated in pulmonary stenosis.

\section*{Tricuspid valve}

Tricuspid regurgitation (TR) is a common finding in asymptomatic patients. The most common cause of TR is impaired valve coaptation caused by dilatation of the RV or of the tricuspid annulus due to left-sided heart disease such as congenital heart defects, and cardiomyopathy, which can lead to pulmonary hypertension (29). For the TOE assessment of TR, the following views should be obtained: 4-chamber view, RV inflow–outflow view at the mid-oesophageal level and transgastric RV inflow and tricuspid short-axis views. Assessment of TR severity is, in principle, similar to MR and has been summarised in the Table 1. Systolic flow reversal in the hepatic veins is the strongest single predictor of the severity of TR (30). Importantly, the absence of systolic flow reversal does not rule out severe TR. Blunted systolic hepatic flow can be seen in abnormal RA and RV compliance, AF and elevated RA pressure. When describing severe TR, the echocardiographer should include in the report the assessment of RA and RV, IVC and hepatic veins and the presence of the systolic bowing of the interatrial septum towards the LA.

Tricuspid stenosis is the least common of the valvular stenosis, and the evaluation of TS is done using the CW Doppler method as described for MS.

\section*{A roadmap for evaluation of prosthetic valves}

Approximately 290,000 prosthetic heart valves are implanted each year worldwide, and this number is estimated to triple to over 850,000 by 2050 (31). The specific flow pattern and imaging features of prosthetic heart valves pose major challenges for the Doppler echocardiographic assessment of structure and function. Consequently, a comprehensive approach that integrates several semi-quantitative and quantitative parameters obtained from multiple views of valve is necessary to assess the prosthetic valve dysfunction (Fig. 2).

By design, almost all prosthetic valves are obstructive. The guidelines suggest that the first postoperative transthoracic echocardiography should be performed 3–12 weeks after surgery (when the haemodynamic status has stabilized and the chest wound has healed),
as the baseline for further follow-up and monitoring of the complications (32). Patients with bioprosthetic valve should be screened by TTE every year after 5 years after their valve implantation. For mechanical valves, routine annual echocardiography is not indicated unless there is high clinical suspicion of complications (32). Prosthesis–patient mismatch (PPM) occurs when the valve EOA of a normally functioning prosthesis is too small in relation to the patient’s body size, and thus, cardiac output requirements, resulting in abnormally high postoperative velocities and gradients (33). To identify the PPM, the EOA of the prosthesis is divided by the patient’s body surface area. Severe PPM is identified when indexed EOA ≤0.65 cm²/m² for aortic and ≤0.9 cm²/m² for mitral prostheses.

Pathologic obstruction of the prosthetic valve may be caused acutely by thrombosis or endocarditis vegetations or by chronic processes such as pannus formation or calcific degeneration of bioprosthetic valve leaflets (structural valve degeneration). To identify the prosthetic valve stenosis, the EOA measured in the patient needs to be compared with the normal reference value of EOA for the model and size of prosthesis that has been implanted (BSE EchoCalc app, (32)). Assessment of severity of prosthetic regurgitation is more complex than in native valves, due to the high prevalence of paravalvular regurgitation and complex, eccentric and irregular jets. Additionally, most of the mechanical prostheses have normal patterns of so-called ‘washing jets’, which are short in duration, narrow and symmetrical. TOE plays an important role in the detection and localisation of prosthetic regurgitation and in demonstrating the surrounding anatomy.

Quantitative methods, such as the proximal isovelocity surface area (PISA), are often not feasible when assessing regurgitation in prosthetic valves due to the problems with applying these methods in situations with complex and multiple jets (11). As an alternative, in such cases we can use the Doppler method estimate of the regurgitant volume. This is done by calculating the difference between the stroke volume measured in the right ventricular outflow tract or at the mitral annulus.

Percutaneous repair of the paravalvular leak

Percutaneous repair of the paravalvular leak (PVL) is an alternative for patients at high operative risk for redo valve replacement. Echocardiographic assessment is essential in patient selection and helps to exclude such contraindications to the percutaneous leak closure such as active infection, valve instability and intracardiac thrombus. Although 2D TOE is used in the initial assessment of the paravalvular regurgitation, 3D echocardiography with multiplane reconstruction is superior in all stages of peri-procedural management. In particular, real-time 3D colour plays an important role in the assessment of procedural success. The clock face is commonly used to describe the location of the PVL. The nomenclature of medial, lateral, anterior and posterior location is also commonly used to characterise the position. TOE allows description of the orifice shape and some assumptions about the size of the PVL, which is essential in the choice of the closure device. TOE guidance is necessary in using the transseptal system and in the deployment of the device. At the end of the procedure, TOE should show mobile valve leaflets and unobstructed structures in proximity to the device.

The role of TOE in management of patients with endocarditis

The high spatial and temporal resolution of the TOE probe allows evaluation of thin and highly mobile structures; TOE is therefore a key imaging modality in assessment of infective endocarditis. It allows the detailed description of size, attachment site and mobility of vegetations and the consequences of infective endocarditis such as abscess and fistula formation in the peri-valvular area, pseudoaneurysms, perforations and chordal rupture. TOE is mandated in assessing prosthetic valves for suspected endocarditis (34). 3D TOE may be superior to 2D imaging in endocarditis because it is able to clearly delineate components of both mechanical and bioprosthetic valves; furthermore, 3D imaging overcomes the challenge of acoustic shadowing commonly seen in 2D imaging of prosthetic valves. 3D echocardiography, with its ability to provide a comprehensive anatomical assessment of the entire valve, is better in distinguishing between a vegetation and the suture material. The en face view is particularly helpful in identifying the valve dehiscence, fistulas and paravalvular leaks as complications of infective endocarditis. It is, however, important to note that due to its higher frame rate, 2D echocardiography is more reliable than 3D when assessing small and very mobile vegetations.

Stroke complicates about 10% of cases of infective endocarditis and represents one of the most severe complication associated with an increased morbidity and mortality (35). Infection of prosthetic valves,
mitral valve and due to aggressive bacteria, such as *Staphylococcus aureus*, is associated with the highest risk of embolization (36). Most stroke-related infective endocarditis happens in the initial phase of disease (36, 37) and thus, an echocardiogram is mandatory in all cases where there is a high clinical suspicion of infective endocarditis. Both the size and mobility of the vegetation have been associated with an increased risk of embolism. Most emboli are fragments of vegetations, and the risk of embolization increases with large vegetations (>10 mm).

**Future perspectives in TOE**

Until relatively recently, an important limitation of 2D echocardiography was that the images generated of the pathology and surrounding anatomy were sometimes difficult to interpret. High-quality, real-time 3D TOE allows visualisation of complex valvular anatomy from any spatial point. This characteristic has so far proven beneficial to an array of procedures, including surgical management of mitral valve repair (including robotic mitral valve repair); nonsurgical mitral procedures such as edge-to-edge mitral repair; transcatheter closure of the paraprosthetic leaks and evaluation of aortic annulus for transcatheter aortic valve implantation. Real-time 3D TOE also offers an important additional dimension in the echocardiographic evaluation of prosthetic valves. Moreover, 3D or even 4D printing has promised to revolutionise the management of valve disease as printing of highly personalised replacement valves may be possible based on the 3D echo images acquired in the future, thus eliminating problems with poorly fitted prosthesis.

Another approach, which is gaining increased popularity, is hybrid cardiac imaging, which uses the principle of combining images obtained with two different imaging modalities to improve diagnostic accuracy. The majority of cardiac hybrid imaging is done by fusion of static rather than dynamic images, most commonly with CT/SPECT images. Currently, only the combination of transoesophageal echocardiography with fluoroscopy allows real-time image fusion of high-quality moving images for improved diagnostic accuracy during structural heart disease interventions. Future developments in hybrid imaging may include fusion techniques to combine CT, nuclear, CMR or TOE images, which may further enhance the diagnostic power of TOE.

**Conclusion**

In this review, we described both established and new 2D and 3D TOE techniques in the management of valvular heart disease. By summarising current guidelines and highlighting areas that remain controversial, we hope we provided a comprehensive overview of the modern and yet evolving role of TOE in general cardiology.

**Declaration of interest**

The authors declare that there is no conflict of interest that could be perceived as prejudicing the impartiality of this review.

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